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**Siebertstrasse 4**

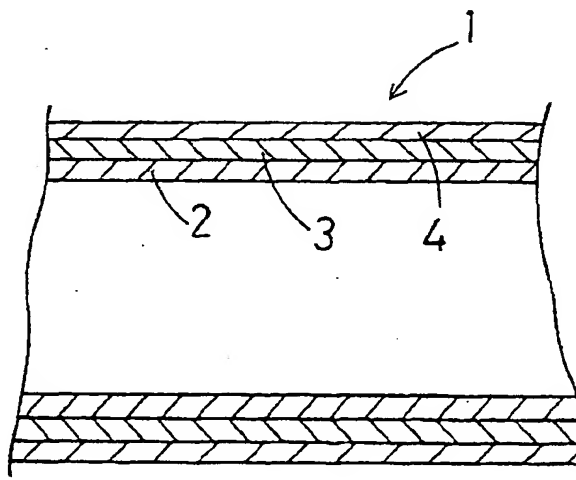
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(54) **A catheter**

(57) The object of the present invention is to present a catheter which can be safely inserted into the body and easily operated in said body. To attain this object, a catheter whose wall has a polylayer structure with more than three layers is provided in the present invention. In said catheter, the mechanical property changes gradually from inside layer to outside layer to obtain the min-

imum difference of the mechanical property between a pair of layers attaching to each other, so that high inter-laminate strength is guaranteed and stress concentration is avoided. Further, in the case where the metal reinforcement is wound on the inner layer to obtain high rigidity, a catheter has a smooth surface without unevenness.

**Fig. 1**



## Description

[0001] The present invention relates to a catheter used for diagnosis or therapeutics.

[0002] A catheter used for diagnosis or therapeutics is guided by guide wire from the outside of the body into the blood vessel, the trachea, the gonaduct, the ureter, etc. to reach a part to be treated to perform diagnosis or therapeutics. Accordingly, said catheter should be flexible enough to bend freely in the blood vessel etc. and not to injure the wall of the blood vessel etc. while said catheter should have a good torque transmission property and said catheter should be rigid enough for the good torque transmission property.

[0003] Hitherto, to solve said antinomy, catheters consisting of a base part having enough rigidity to transmit the torque and an end part having flexibility to bend freely have been presented (TOKKAISHo 60-31765, Japanese Patent No. 2523405).

[0004] In TOKKAISHo 60-31765, the tube wall of the catheter has a two-layer structure consisting of an inner tube part and an outer tube part and when the flexibility of said inner tube part is set to be smaller than the flexibility of said outer tube part, the thickness of said inner tube part in said base part is set to be larger than the thickness of said inner tube part in said end part, and when the flexibility of said inner tube part is set to be larger than the flexibility of said outer tube part, the thickness of said outer tube part in said base part is set to be larger than the thickness of said outer tube part in said end part to give said base part high rigidity for a good torque transmission property and said end part high flexibility to bend freely.

[0005] Further, in Japanese Patent No. 2523405, a catheter having a rigid base part and a flexible end part is provided wherein the glass transition temperature of the organic material of said base part is set to be higher than the glass transition temperature of the organic material of said flexible end part and further, a metal reinforcement is wound on the outside of said base part and still further, a synthetic resin coating is applied on said reinforcement to give said base part high rigidity.

[0006] Said catheter of TOKKAISHo 60-31765 has faults in that the flexibility of said inner tube part is much different from the flexibility of said outer tube part, resulting in poor interlaminar strength between said inner tube part and said outer tube part and said catheter is easily folded by stress concentration.

[0007] Further, said catheter of Japanese Patent No. 2523405 has a fault in that the unevenness of the metal reinforcement appears on the surface of synthetic resin coating.

[0008] Accordingly, an object of the present invention is to present a catheter consisting of a base part having enough rigidity for a good torque transmission property and an end part having enough flexibility to bend freely.

[0009] To attain this object, a catheter whose tube wall has a polylayer structure with more than three layers is

presented in the present invention.

[0010] In the present invention, said catheter consists of a base part and an end part, and said base part is reinforced by a metal reinforcement arranged on the outside of the inner layer to give said base part enough rigidity.

[0011] It is preferable that the glass transition temperature of said polylayer becomes gradually higher from the inside to the outside and the glass temperature of the outer layer is equal to or lower than the bodily temperature.

[0012] Further, it is preferable that said catheter has a three layer structure consisting of an inner layer, a middle layer, and an outer layer and said metal reinforcement arranged on the outside of the inner layer is covered with said middle layer and said middle layer and outer layer consist of the same material.

[0013] Still further, it is preferable that the material of said outer layer is in the rubbery state at the bodily temperature when said catheter is inserted into the body, the bending modulus of elasticity of said material is more than 1000 kgf/cm<sup>2</sup> at a temperature close to the bodily temperature, the material of said inner layer keeps the glassy state at the bodily temperature when said catheter is inserted into the body, and the bending modulus of elasticity of said material is more than 2500 kgf/cm<sup>2</sup> at 23°C.

[0014] Still further, it is preferable that 15000 kgf/cm<sup>2</sup>  $\geq G_1 \geq 8000$  kgf/cm<sup>2</sup> and 3500 kgf/cm<sup>2</sup>  $\geq G_3 \geq 1000$  kgf/cm<sup>2</sup> wherein  $G_1$  is the bending modulus of elasticity of said inner layer and  $G_3$  is the bending modulus of elasticity of said outer layer.

[0015] Still further, it is preferable that said catheter consists of a base part and an end part, and the thickness of the inner layer of said base part is larger than the thickness of the inner layer of said end part.

[0016] The invention will be described with reference to preferred embodiments and the drawings, in which:

[0017] Figure 1 to Figure 3 show an embodiment of the present invention.

[0018] Figure 1 is the enlarged partial cross sectional view of a catheter.

[0019] Figure 2 is the whole side view of said catheter.

[0020] Figure 3 is the cross sectional view of the boundary part between the base part and the end part.

[0021] Figure 4 and 5 show the other embodiment of the present invention.

[0022] Figure 4 is a perspective view to illustrate the manufacturing process of a catheter.

[0023] Figure 5 is the enlarged cross sectional view of the boundary part between the base part and the end part.

[0024] Figure 1 to Figure 3 relate to an embodiment of the present invention. A catheter (1) shown in Figures has a tube wall having a three-layer structure which consists of an inner layer (2), a middle layer (3) and an outer layer (4) and assuming the bending modulus of elasticity of said inner layer (2) at a temperature close to the bodily

temperature is  $G_1$ , the bending modulus of elasticity of said middle layer (3) at a temperature close to the bodily temperature is  $G_2$ , and the bending modulus of elasticity of said outer layer (4) at a temperature close to the bodily temperature is  $G_3$ ,  $15000 \text{ kgf/cm}^2 \geq G_1 \geq G_2 \geq G_3 \geq 1000 \text{ kgf/cm}^2$ , preferably  $15000 \text{ kgf/cm}^2 \geq G_1 \geq 8000 \text{ kgf/cm}^2$ ,  $6000 \text{ kgf/cm}^2 \geq G_2 \geq 4000 \text{ kgf/cm}^2$ ,  $3500 \text{ kgf/cm}^2 \geq G_3 \geq 1000 \text{ kgf/cm}^2$  and the material of said inner layer (2) keeps the glassy state at the bodily temperature when said catheter (1) is inserted into the body and the material of said outer layer (4) is in the rubbery state at the bodily temperature when said catheter (1) is inserted into the body. Accordingly, the glass transition temperature  $T_{G1}$  of said inner layer (2) is set to be higher than the bodily temperature  $T_0$  ( $T_{G1} > T_0$ ) and the glass transition temperature  $T_{G3}$  of said outer layer (4) is set to be equal to or lower than the bodily temperature  $T_0$  ( $T_{G3} \leq T_0$ ). Wherein  $T_0$  is, for example, in the range between  $35$  to  $37^\circ\text{C}$  but may reach  $40^\circ\text{C}$  when the body has hyperthermia.

[0025] Further, in the case where the material of each layer of said catheter (1) is an incomplete amorphous material, it is desirable that the crystallinity of said outer layer is equal to or lower than 30% at the bodily temperature  $T_0$ .

[0026] The material of said catheter is, for example, urethane elastomers, styrene elastomers, ester elastomers, olefin elastomers, amido elastomers, fluoroelelastomers or mixtures of two or more kinds of these elastomers. A filler having radiopacity such as barium sulfate and the like is preferably added to said elastomers in an amount between 30 to 50% by weight so that a catheter can be detected by radiography.

[0027] As shown in Figure 2, said catheter (1) consists of a base part (1A) and an end part (1B), and generally it is preferable that said base part (1A) has high rigidity and said end part (1B) has flexibility.

[0028] To give said base part (1A) high rigidity, and said end part (1B) flexibility, the thickness  $t_{A1}$  of said inner layer (2) of said base part (1A) is set to be larger than the thickness  $t_{B1}$  of said inner layer (2) of said end part (1B), and the thickness  $t_{A3}$  of said outer layer (4) of said base part (1A) is set to be less than the thickness  $t_{B3}$  of said inner layer (2) of said end part (1B). Concretely, in said base part (1A),  $0.18 \text{ mm} \leq t_{A1} \leq 0.19 \text{ mm}$ ,  $0.03 \text{ mm} \leq t_{A3} \leq 0.05 \text{ mm}$ ,  $t_{A1} > t_{A3}$ , and in said end part (1B),  $0.07 \text{ mm} \leq t_{B1} \leq 0.09 \text{ mm}$ ,  $0.14 \text{ mm} \leq t_{B3} \leq 0.15 \text{ mm}$ ,  $t_{A1} < t_{A3}$  and  $t_{A1} > t_{B1}$ ,  $t_{A3} < t_{B3}$ .

[0029] Total thickness of the tube wall of said catheter (1) is generally 0.6 to 0.7 mm so that the thickness  $t_{A2}$  of said middle layer (3) of said base part (1A) is  $t - t_{A1} - t_{A3}$  and the thickness  $t_{B2}$  of said middle layer (3) of said end part (1B) is  $t - t_{B1} - t_{B3}$  ( $t_{A2} = t - t_{A1} - t_{A3}$ ,  $t_{B2} = t - t_{B1} - t_{B3}$ ).

[0030] When said catheter (1) of this embodiment is inserted into the body and effected by the bodily temperature, the bending modulus of elasticity  $G_3$  of said outer layer (4) is set to be low, such as  $3500 \text{ kgf/cm}^2 \geq$

$G_3 \geq 1000 \text{ kgf/cm}^2$ , and said outer layer (4) is set to be in the rubbery state, so that said catheter (1) has enough flexibility to bend easily following the curve shape of the blood vessel and said outer layer (4) can follow a curve having a small curvature radius without cracking or breaking.

[0031] Further, in the case of the curve having a small curvature radius, if the crystallization of said outer layer (4) by tensile stress advances, said outer layer (4) may harden to be in danger of cracking or breaking while said outer layer (4) of said catheter (1) of this embodiment shows no advance of the crystallization by tensile stress.

[0032] Further, when the tube is molded by extrusion using a rigid material, sinks may be formed on the surface of the tube. However, in this embodiment, the inside layer of said rigid material is covered with the outside layer of a soft material having good fluidity filling up said sinks of the inside layer to obtain a catheter having a smooth surface without unevenness. If a catheter has an uneven surface, it is feared that the thrombus adheres to said catheter resulting in the difficulty of inserting said catheter into the blood vessel.

[0033] As above described, said outer layer of said catheter of this embodiment is so soft that safety in diagnosis or therapeutic is guaranteed without injuring the blood vessel and the like.

[0034] Further, as said inner layer (2) of said catheter (1) of this embodiment has a high bending modulus of elasticity  $G_1$  such as  $15000 \text{ kgf/cm}^2 \geq G_1 \geq 8000 \text{ kgf/cm}^2$  and the glass temperature of said inner layer (2) is set to be higher than the bodily temperature, said catheter (1) has an enough torque transmission property when said catheter (1) is inserted into the body and easy operation for diagnosis or therapeutic is guaranteed.

[0035] Still further, in said catheter (1) of this embodiment, as the bending modulus of elasticity becomes gradually higher from the inner layer to the outer layer, the difference of the mechanical property between a pair of layers attaching to each other may become small, resulting in high interlaminar strength and, folding by stress concentration is effectively avoided.

[0036] Figure 4 and Figure 5 show the other embodiment of the present invention.

[0037] As shown in Figure 4, the outside of a core bar (16) is covered with a melted material or a solution of a material by coating or extrusion to form an inner layer (12) by cooling or drying and then a tubular metal net is wound on said inner layer (12) in a base part (11A) as a metal reinforcement (15). The same material as used in the prior embodiment is used in this embodiment.

[0038] Said metal reinforcement (15) is covered with a middle layer (13) and further said middle layer (13) is covered with an outer layer (14). Said middle layer (13) and said outer layer (14) may be formed by coating or extrusion using the same material as used in the prior embodiment. Preferably, the same material is used for said middle layer (13) and said outer layer (14) to obtain

higher interlaminar strength.

[0039] As shown in Figure 5, a catheter (11) having three layer structure consisting of said inner layer (12), and middle layer (13) and said outer layer (14) is manufactured by the process as above described. Said base part (11A) has high rigidity by inserting said metal reinforcement (15) between said inner layer (12) and said middle layer (13) to obtain a good torque transmission property. Further, said catheter (11) has a smooth surface without unevenness since unevenness of the surface of said middle layer caused by unevenness of said metal reinforcement is filled by said outer layer (14), and said end part (11B) has enough flexibility since no metal reinforcement is inserted in the end part (11B).

[0040] The catheter of the present invention has a polylayer structure with more than three layers and in the case where the mechanical property changes gradually from inside layer to outside layer to obtain the minimum difference of the mechanical property between a pair of layers attaching to each other, high interlaminar strength is guaranteed and stress concentration is avoided. Further, in the case where the metal reinforcement is used to obtain high rigidity, a catheter having a smooth surface without unevenness is obtained when said metal reinforcement is inserted between a pair of layers.

#### Claims

1. A catheter whose tube wall has a polylayers structure with more than three layers.
2. A catheter of Claim 1, wherein said catheter consists of a base part and an end part, said base part is reinforced by a metal reinforcement arranged on the outside of the inner layer.
3. A catheter of Claim 1 or 2, wherein the glass transition temperature of said polylayer becomes gradually higher from the inside to the outside and the glass temperature of the outer layer is equal to or lower than the bodily temperature.
4. A catheter of Claim 2 or 3, wherein said catheter has a three layer structure consisting of an inner layer, a middle layer, and an outer layer and said metal reinforcement arranged on the outside of the inner layer is covered with said middle layer and said middle layer and outer layer are made of the same material.
5. A catheter of any of claims 1 to 4, wherein the material of said outer layer is in the rubbery state at the bodily temperature when said catheter is inserted into the body, the bending modulus of elasticity of said material is more than 1000 kgf/cm<sup>2</sup> at a temperature close to the bodily temperature, the material of said inner layer keeps the glassy state at the bodily temperature when said catheter is inserted into the body, and the bending modulus of elasticity of said material is more than 2500 kgf/cm<sup>2</sup> at 23°C.
6. A catheter of claim 4, wherein  $15000 \text{ kgf/cm}^2 \geq G_1 \geq 8000 \text{ kgf/cm}^2$  and  $3500 \text{ kgf/cm}^2 \geq G_3 \geq 1000 \text{ kgf/cm}^2$  wherein  $G_1$  is the bending modulus of elasticity of said inner layer and  $G_3$  is the bending modulus of elasticity of said outer layer.
7. A catheter of Claim 5 or 6, wherein said catheter consists of a base part and an end part, the thickness of the inner layer of said base part is larger than the thickness of the inner layer of said end part.

Fig. 1

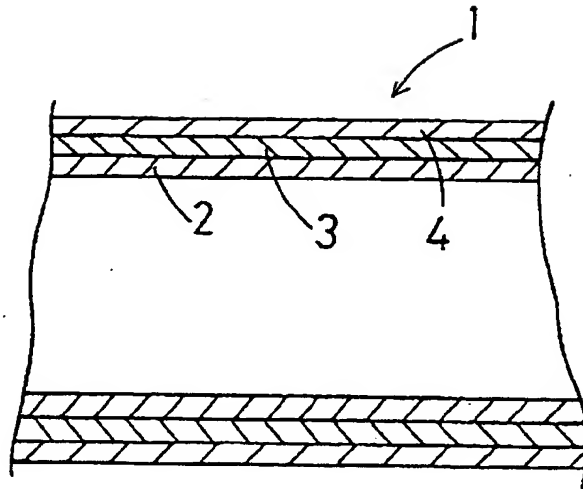


Fig. 2

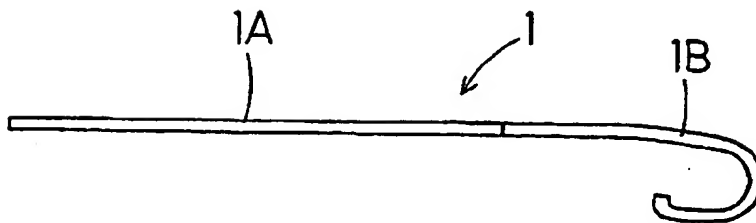


Fig. 3

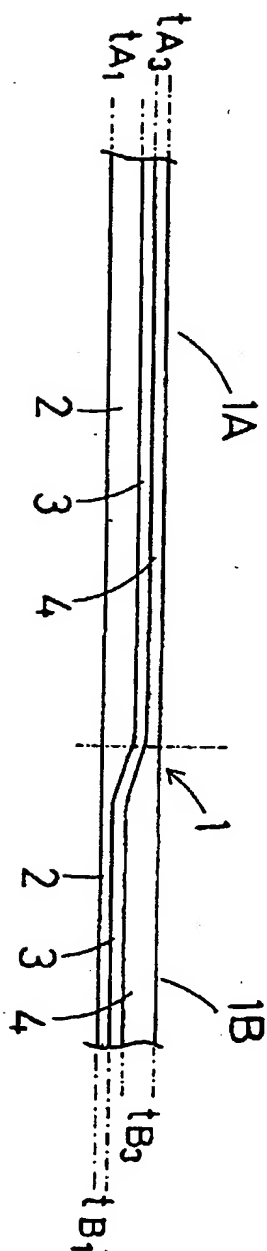


Fig. 4

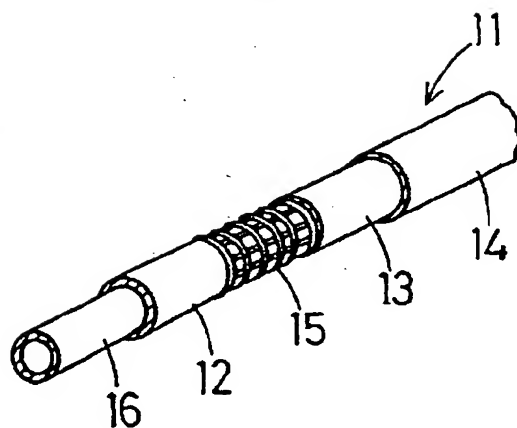
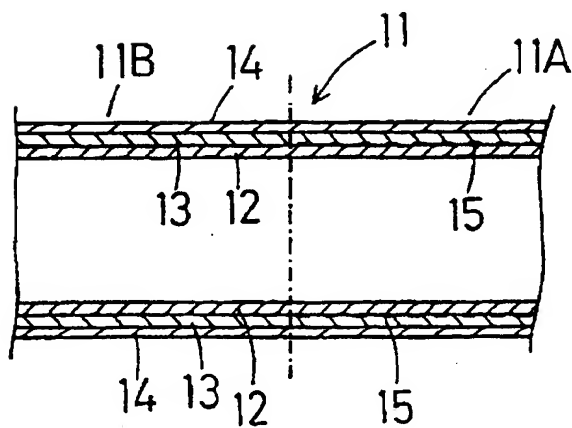
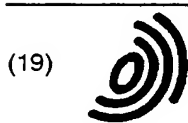


Fig. 5









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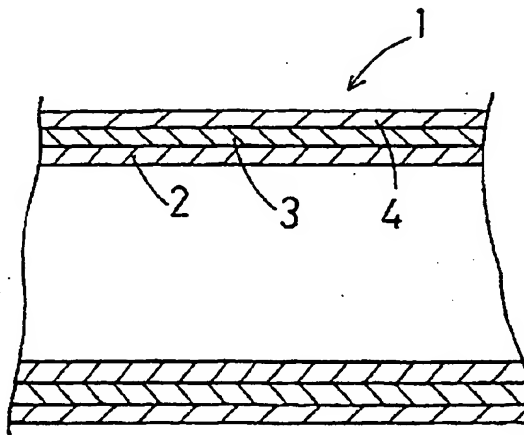
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(54) **A catheter**

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imum difference of the mechanical property between a pair of layers attaching to each other, so that high inter-laminate strength is guaranteed and stress concentration is avoided. Further, in the case where the metal reinforcement is wound on the inner layer to obtain high rigidity, a catheter has a smooth surface without unevenness.

**Fig. 1**





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## EUROPEAN SEARCH REPORT

Application Number  
EP 99 10 1045

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X	WO 96 33763 A (TARGET THERAPEUTICS) 31 October 1996 (1996-10-31) * page 17, line 6 - page 19, line 6 * * page 24, line 29 - page 26, line 4 * * figures 8-10 *	1, 2, 4	A61M25/00
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The present search report has been drawn up for all claims			
Place of search		Date of completion of the search	Examiner
THE HAGUE		18 November 1999	Schönleben, J
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

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